

1 REVIEW ARTICLE

2 **Direct electrical brain stimulation of human memory:** 3 **lessons learnt and future perspectives**

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5 **Abstract**

6 Modulation of cognitive functions supporting human declarative memory is one of the grand
7 challenges of neuroscience, and of vast importance for a variety of neuropsychiatric,
8 neurodegenerative and neurodevelopmental diseases. Despite a recent surge of successful
9 attempts at improving performance in a range of memory tasks, the optimal approaches and
10 parameters for memory enhancement have yet to be determined. On a more fundamental
11 level, it remains elusive how delivering electrical current in a given brain area leads to
12 enhanced memory processing. Starting from the local and distal physiological effects on
13 neural populations, the mechanisms of enhanced memory encoding, maintenance,
14 consolidation, or recall in response to direct electrical stimulation are only now being
15 unraveled. With the advent of innovative neurotechnologies for concurrent recording and
16 stimulation intracranially in the human brain, it becomes possible to study both acute and
17 chronic effects of stimulation on memory performance and the underlying neural activities. In
18 this review, we summarize the effects of various invasive stimulation approaches for
19 modulating memory functions. We first outline the challenges that were faced in the initial
20 studies of memory enhancement and the lessons learned. Electrophysiological biomarkers
21 are then reviewed as more objective measures of the stimulation effects than behavioral
22 outcomes. Finally, we classify the various stimulation approaches into continuous and phasic
23 modulation with open or closed loop for responsive stimulation based on analysis of the
24 recorded neural activities. Although the potential advantage of closed-loop responsive
25 stimulation over the classic open-loop approaches is inconclusive, we foresee the emerging
26 results from ongoing longitudinal studies and clinical trials to shed light on both the
27 mechanisms and optimal strategies for improving declarative memory. Adaptive stimulation
28 based on the biomarker analysis over extended periods of time is proposed as a future
29 direction for obtaining lasting effects on memory functions. Chronic tracking and modulation
30 of neural activities intracranially through adaptive stimulation opens tantalizing new avenues

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1 to continually monitor and treat memory and cognitive deficits in a range of brain disorders.
2 Brain co-processors created with machine-learning tools and wireless bi-directional
3 connectivity to seamlessly integrate implanted devices with smartphones and cloud
4 computing are poised to enable real-time automated analysis of large data volumes and
5 adaptively tune electrical stimulation based on electrophysiological biomarkers of behavioral
6 states. Next generation implantable devices for high-density recording and stimulation of
7 electrophysiological activities, and technologies for distributed brain-computer interfaces are
8 presented as selected future perspectives for modulating human memory and associated
9 mental processes.

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24
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1 **Challenges of probing declarative memory with direct brain stimulation**

2 Our ability to form, store and recall declarative memories has been one of the most
3 challenging functions to map and modulate in the human brain. Unlike the implicit types of
4 memory for motor skills, habits or emotional responses, which can be localized and treated in
5 specific cortical, thalamic and basal ganglia regions ¹, explicit memory functions are
6 distributed across widespread sensorimotor, limbic and executive networks. Declarative
7 memory involves multiple complex cognitive functions (see Box 1, Complexity of memory
8 functions) but minimally requires the encoding and conscious recollection of unique episodes
9 or general facts, involving multisensory representations in specific contexts of time and
10 space. This function requires engagement of complex physiological processes across several
11 levels of brain organization – from single cells to local assemblies and large-scale distributed
12 networks – in multiple cortical and subcortical brain regions. Intracranially implanted (i.e.,
13 invasive) electrodes provide a rare but powerful opportunity to probe the role of specific
14 regions in declarative memory and other cognitive functions ²⁻⁶. Direct electrical stimulation
15 (DES) using these intracranial electrodes can test causative roles of distinct anatomical
16 targets and physiological processes in modulating human declarative memory performance.

17
18 Mapping the brain regions involved in processing declarative memories sounds easier than it
19 actually is. The classic reports of subjective recollection or ‘re-experiencing’ specific
20 episodes from the past during intra-operative DES ^{15,16}, identified sparsely distributed
21 locations of the effective stimulation sites across associative cortical areas. A recent thorough
22 investigation of cortical DES ¹⁷ showed that such complex subjective responses are less
23 frequent and less consistent than simple sensory or motor responses that are commonly
24 localized in the clinical setting of cortical mapping. This important study showed that
25 memory-related phenomena could be elicited by stimulating cortical areas of the limbic and
26 salience networks. Notably, hippocampal electrodes were not stimulated in this study.

27
28 While this study shows that higher cognitive functions such as declarative memory rely on
29 distributed networks rather than individual brain regions, DES is not confined to focal effects
30 either but is thought to elicit widespread brain responses. In fact, even microstimulation
31 preferentially activates widely distributed neuronal assemblies more than local cell
32 populations in the immediate vicinity of the stimulating electrode ¹⁸. The electrophysiological
33 responses to DES have recently been more systematically studied in the human brain ¹⁹⁻²²,

1 confirming both local and distal effects of macro-electrode stimulation. DES-induced
2 changes in the spectral activities were observed both close to the stimulation site on the
3 neighboring electrode contacts (4-10 mm) and away in remote cortical areas (>10 cm away).
4 Still, even these recent studies that used the same experimental dataset found various and
5 often opposite effects in neural activities of particular frequencies of the human intracranial
6 EEG (iEEG) spectrum, revealing challenges for consistent signal processing and data
7 analysis. The effects of the frequency or amplitude of the stimulation current or the proximity
8 to the white matter tracts²³ are also subjects of pending debate. Eliciting consistent neural
9 responses in particular iEEG frequency bands, for instance theta or gamma, would be pivotal
10 for predicting the effects on memory processing. The recent studies prove how challenging it
11 is even to determine the most effective parameters of current frequency or amplitude to
12 obtain a desired effect on the iEEG activities underlying successful memory performance
13 ^{21,22,24,25}.

14
15 One would imagine that electrical stimulation of a given patch of the cortex consistently
16 elicits the same neurophysiological and behavioral responses every time it is applied. In
17 practice, however, DES evokes a complex response of the underlying neural networks that is
18 reflected in heterogeneity of the neural, cognitive, and behavioral effects²⁶, even in the case
19 of simple sensory or motor functions. This variability may derive from a number of different
20 factors. First, the excitability of the stimulated brain region may undergo substantial
21 fluctuations (e.g.^{27,28}), which was found to be reflected by the phase of ongoing low-
22 frequency oscillations (in particular, in the theta frequency range, e.g.²⁹). These local
23 excitability fluctuations may, however, be driven in remote areas that process variable
24 degrees of attentiveness, drowsiness, or task engagement. Second, physiological activity
25 patterns in single brain regions may reflect different variables depending on current goals, an
26 effect known as “mixed selectivity” (e.g.,³⁰). Finally, effects of repetition suppression (or
27 repetition enhancement) may lead to more sparse (or more pronounced, respectively)
28 responses due to changes in the tuning functions of individual neurons or neural assemblies.

29
30 If predicting the electrophysiological responses to DES is challenging enough, then how
31 much more unpredictable are the cognitive and behavioral outcomes? This was clearly
32 demonstrated in the case of mesial temporal lobe stimulation to modulate spatial memory
33 performance. Positive effects that were originally reported in a pioneering study with 6

1 epilepsy patients ³¹ failed to be reproduced in a similar behavioral paradigm with a larger
2 group of patients ³², despite an overall match of the anatomical location as well as the
3 parameters of stimulation. Precise anatomical location, including proximity to white matter
4 tracts, were proposed as a key factor for predicting the effects on memory performance ^{23,33,34}
5 along with others that may account for inconsistencies observed across the early studies ^{34–36}.

6
7 Most of the early studies reported the behavioral effects either in individual cases ^{37–39} or
8 small groups of patients ^{31,40–50}, where significant effects of DES were found only in some
9 individual patients or on a group level - often inconsistent across studies. The need for more
10 robust and reproducible results can be addressed with larger multi-center studies. One of the
11 first such studies yielded break-through data (Fig. 1) showing a robust positive effect of DES
12 in the lateral temporal cortex on verbal memory performance observed both on the level of
13 single patients and the group ²⁴. This effect was confirmed in the same project using a closed-
14 loop stimulation approach with another group of patients ²⁵. Thus, two studies with approx.
15 50 patients altogether showed consistent effects of DES in the lateral temporal cortex but not
16 the other brain regions, including the hippocampus. Surprisingly, however, a positive effect
17 in a similar paradigm was subsequently reported with analogous stimulation in the
18 hippocampus ⁵¹. Hence, even though increasing the study size makes the results more robust
19 and reproducible across large studies, it may not necessarily generalize to other smaller
20 studies.

21
22 More studies have been conducted with non-invasive brain stimulation methods (see Box 2
23 ‘Overview of non-invasive brain stimulation approaches’) to modulate memory functions.
24 These, however, were also challenged by the issues of mixed effects, lack of consistency, and
25 heterogeneity of the study designs and stimulation paradigms ^{36,52–54}. A systematic review of
26 the studies confirmed moderate effects limited to working, episodic and procedural memory
27 ⁵⁵. One recent study showed a 10-20% enhancement in verbal memory ^{56,57}, which was in the
28 same range of magnitude as the DES studies ^{24,25}. Duration of the stimulation-induced
29 performance in these was limited to only acute immediate effects. A more recent study has
30 shown promising results of chronic effects with a non-invasive stimulation ^{58,59} (see also
31 below ‘Biomarkers of neuromodulation’).

1 **Biomarkers of neuromodulation**

2 To reliably predict the behavioral effects of DES, one would first need validated biomarkers
3 of cognitive processes that may be targeted via neuromodulation. The large study on memory
4 DES described above correlated the effects of stimulation on memory performance and on
5 iEEG activities in the gamma frequency range induced by memory encoding at specific
6 sensory and associative cortical locations⁶⁵. Positive modulation of gamma power with DES
7 in the lateral temporal cortex, i.e. more power when stimulated, was associated with
8 improved memory performance, whereas negative modulation with DES in the mesial
9 temporal lobe, i.e. less power when stimulated, correlated with memory impairment. These
10 results were congruent with the opposite effects of DES in the two structures^{24,25,32,66,67},
11 revealing a positive and a negative neuromodulation, respectively (Fig. 1). It should,
12 therefore, be possible to predict the behavioral outcomes of DES based on its effect on iEEG
13 activities (i.e., gamma power). Reversely, it may be possible to deliver stimulation during less
14 beneficial states and thereby modify these brain states into more beneficial states. This
15 approach was taken in several previous studies, which first used pattern classification
16 analyses to identify biomarkers of memory formation and then stimulated in trials showing
17 poor-functioning states^{25,68,69}. In these studies, DES (charge-balanced, square-wave
18 stimulation at 50-200 Hz, 0.3 ms pulse width, and 1.0-3.0 mA amplitude) applied when
19 stimuli were presented for encoding during identified poor states improved recall
20 performance in the task. Even though the behavioral effects were only moderate, these
21 pioneering studies set a new standard for employing machine-learning tools to validate iEEG
22 biomarkers and identify optimal time points for DES.

23
24 Previous smaller studies described particular electrophysiological activities that were
25 modulated by DES without validating a possible biomarker. For instance, enhanced
26 performance in a spatial memory task observed with DES in the entorhinal cortex was
27 associated with resetting of the iEEG theta rhythm in the hippocampus³¹. Hippocampal
28 stimulation that enhanced performance in a verbal memory task was found to modulate iEEG
29 power of the hippocampal theta rhythm^{51,70}. Amygdala stimulation, which led to improved
30 memory for images, modulated theta and gamma iEEG coherence and phase-amplitude
31 coupling between the mesial temporal lobe structures⁷¹. Other studies showed evoked
32 responses, which may correspond to low-frequency power increases and/or phase resetting,
33 or general activation of a distinct brain region in response to effective DES^{38,40,43,44}. None of

1 these studies, however, demonstrated a causal relationship between a neural activity and
2 modulation of behavior, e.g. through an intervention that would specifically target the activity
3 and cause either an enhancement or an impairment in memory performance, which would be
4 needed to validate an electrophysiological biomarker predictive of both positive and negative
5 effects of DES.

6
7 More direct evidence for the causal relationship is provided by targeting a neural activity
8 pattern with DES and predicting behavioral outcomes. One of the first such studies tested the
9 effect of synchronous stimulation of two connected mesial temporal lobe structures on
10 memory performance, in an attempt to enhance a previously observed connectivity marker of
11 successful memory formation ^{42,72}. The study found a trend for better memory performance
12 with in-phase stimulation between the structures than with sham or anti-phase stimulation.
13 Although there was no significant memory enhancement, the study pioneered a heuristic
14 approach to testing the effects of DES. A similar approach to synchronous stimulation of the
15 prefrontal and parietal cortical regions was associated with memory enhancement ⁷³.

16
17 These studies suggest that targeting a specific iEEG biomarker of memory processing may be
18 more effective than trying to enhance memory functions only at a level of the observed
19 behavioral change. Physiologically induced activities during memory encoding were
20 specifically used as a target for DES timing and parameter settings to mimic or boost
21 endogenous iEEG activities ^{37,65,74–76}. On the other hand, responding to a biomarker may also
22 result in a neural effect without any observable behavioral counterpart, in particular if the
23 biomarker is not highly specific for memory functions. In fact, a recent study showed a
24 modulation of event-related potentials in a specific subregion of the hippocampus without an
25 effect on task performance ⁷⁷. Thus, the therapeutic potential of targeted amplification or
26 entrainment remains to be clearly demonstrated in case of intracranial studies ⁶¹.

27
28 Another way to test the causal relationship between ongoing brain states and DES effects
29 could be to trigger presentation of the encoded stimuli to the phase of an on-going neural
30 oscillation ⁷⁸. Although electrical stimulation is not involved, this biomarker approach has
31 been repeatedly adopted in targeted memory reactivation studies during sleep, i.e., presenting
32 cues that had been paired with stimuli during previous learning stages during specific phases

1 of slow waves (Ngo et al., 2013). However, this approach may be less feasible during
2 memory formation or retrieval in real-world settings, where the exact timing of stimuli to be
3 encoded or the occurrence of retrieval cues is typically difficult or impossible to control.

4
5 While the timing of stimuli may be difficult to control in ecological settings, a more feasible
6 strategy may be to trigger the timing of DES to specific biomarkers; we now have the tools to
7 trigger and test DES in response to neural activities, which can be analyzed in real-time and
8 in a closed loop of sensing and stimulation. This is one example of *responsive* DES, in which
9 a response in the form of stimulation at particular parameters is controlled by feedback from
10 real-time biomarker analysis. Closed-loop responsive stimulation can be a powerful tool for
11 validating an iEEG biomarker and testing the putative physiological mechanisms of DES
12 modulation of memory processing. The biomarker first needs to be reliably detected together
13 with particular memory processes; then it has to be robustly induced by DES at specific
14 parameters; finally, it should ideally be consistently modulated together with memory
15 performance⁷⁹. This principled approach assumes that DES-mediated modulation of memory
16 functions works by inducing the physiological iEEG activities underlying memory processing
17^{37,80}. However, recent studies of iEEG activities induced by various parameters or patterns of
18 passive DES outside of any cognitive task^{19–22,81} reveal a more complex picture. DES applied
19 at particular frequencies and amplitudes may either induce or suppress neural activities across
20 a range of iEEG frequencies and anatomical locations. For instance, DES at gamma
21 frequencies can actually decrease the power of iEEG activities in the gamma range and at the
22 same time increase the power in the theta range²². There is variability of these passive
23 responses between studies, not to mention the variability between specific cases, as discussed
24 above. Lack of a reliable biomarker may be part of the reason for only moderate effects of
25 biomarker-driven stimulation compared to a *non-responsive* open-loop DES approach^{24,25},
26 which does not use feedback from the neural activities. Closed-loop, biomarker-driven, real-
27 time responsive DES that would outperform simple open-loop stimulation remains yet to be
28 clearly demonstrated. Without validated biomarkers, responsive DES is challenging and
29 difficult to interpret or optimize.

30
31 So far, neither the mechanisms of stimulation nor the neurophysiological basis of biomarkers
32 have been fully elucidated, even for the classic clinical application of deep stimulation in the
33 basal ganglia for movement disorders^{82–85}. Given the complexity of the immediate acute

1 responses that often cannot be expressed with the conventional concepts of neural excitation
2 or inhibition, the term ‘neuro-modulation’ was proposed to express lasting network effects of
3 stimulation⁸⁶. There is a growing body of literature about the effects of stimulation on the
4 molecular, cellular, and behavioral levels⁸⁷. Still, we are only beginning to understand the
5 physiological mechanisms of stimulation and of the biomarkers that should ideally be used to
6 evaluate the effect of stimulation on the level of neural networks. Further research on these
7 questions will be key to understanding and developing new applications for treating specific
8 brain functions. Arguably, even classic deep stimulation in basal ganglia could then be more
9 effective in treating movement disorders, not to mention cognitive DBS approaches such as
10 those used to enhance memory functions^{88,89}.

12 **Various approaches to neuromodulation**

13 There are multiple approaches to modulate memory processing. *Closed-loop* stimulation
14 triggered by online analysis of iEEG signals is but one example of responsive, i.e. biomarker-
15 driven approaches. The non-responsive DES in an *open loop*, where the stimulation is applied
16 at fixed times of cognitive processing or continuously, does not require online biomarker
17 analysis. It can still take advantage of iEEG signal analysis like in case of a multi-center
18 study²⁴, which determined the anatomical targets and parameters of stimulation before an
19 experiment based on offline analysis during task performance without any stimulation.
20 During the experiment, the location (a pair of electrodes in a brain region that showed
21 memory-related spectral power changes) and the parameters of the electrical current
22 (frequency, amplitude, pulse-width and duration that induced the largest iEEG response)
23 were fixed and DES was triggered at predefined times of memory encoding. These were
24 changed, however, after each experiment based on offline biomarker analysis. Even though it
25 was not a responsive closed-loop stimulation *per se*, the approach benefited from the offline
26 biomarker analysis. In the end, the magnitude of the resultant positive effect of open-loop
27 DES on memory performance was like the one obtained in the follow-up study with DES
28 applied in a closed loop^{24,25}. Therefore, the effect of brain stimulation may be robust to
29 various stimulation approaches, where responsive DES is just one example in a range of
30 effective approaches to modulate memory processing.

31

1 Most of the previous studies that reported a positive effect of DES on memory functions were
2 not employing responsive stimulation (Table 1). Many of the initial reports applied electrical
3 current in a particular brain target continuously in time and at fixed parameters^{38–40,42,44–47,90}.
4 This most basic type of stimulation can generally be classified as ‘*continuous*’, in which
5 electrical current is delivered at fixed parameters continuously in time, in contrast to ‘*phasic*’
6 approaches with current delivered only at discrete times, i.e., phasically. The phasic
7 approaches can use both open and closed loop of stimulation, where the former is non-
8 responsive with no need for online signal recordings and the latter is responsive based on
9 feedback analysis of the recorded signals and biomarkers. Closed-loop analysis is typically
10 performed in real-time to close the loop with minimal delays, but the feedback from the
11 analysis can extend over longer periods of time. Extending the loop is especially needed for
12 analysis of longer stretches in recorded data or when intensive computations are required.
13 One good example is seizure prediction and forecasting^{91,92} that uses a long history of, e.g.,
14 circadian rhythms in the recorded signals to perform classification analyses for estimating the
15 probability of seizure occurrence at a present time (prediction) or in future (forecasting)^{93–95}.
16 All in all, it could still theoretically be categorized as a closed-loop responsive stimulation,
17 since DES would ultimately be delivered in response to analysis of the recorded signals – just
18 delayed in time. The various scenarios of closing the loop for a responsive stimulation are
19 summarized in Figure 2, together with distribution of feedback analysis to local and remote
20 computations. Hence, responsive stimulation can be implemented at a range of timescales and
21 technical solutions for closing the loop.

22
23 Included in this basic proposal for categorization of the approaches is another distinction
24 between *acute* and *chronic* modes of delivering electrical current. In the *acute* mode, which is
25 typically applied in a laboratory or clinical environment, DES is only delivered upon demand
26 for a set period of time. This again can be very brief during a particular cognitive process like
27 memory encoding or recall of the open- or closed-loop stimulation (Table 1), which are
28 typically short even though they involve complex and even opposing interactions (see Box 1).
29 Alternatively, stimulation can also extend over a wider timeframe of intense vigilance and
30 cognitive activity like during office hours, regulated manually or adjusted automatically. An
31 example would be switching the stimulation ON at work or at school and OFF during all the
32 other periods of quiet wakefulness, resting and sleep, or vice versa targeting a different
33 consolidation process during sleep. In contrast, the chronic mode, which is typically applied

1 outside of the laboratory or clinical environments, is defined as maintaining a given DES
2 approach over extended time. Notice that both phasic and continuous *categories* of DES
3 approach can be applied in the acute or chronic *mode* (Table 1). A responsive closed-loop
4 DES (*type* of approach) can only be acutely switched on during active wakefulness or only at
5 sleep to modulate sleep-dependent memory consolidation. It can also be chronically switched
6 on - the *category* of stimulation is still phasic (not continuous) and the *type* is responsive but
7 applied in a chronic *mode*. An example of this approach would be responsive stimulation
8 triggered by seizure detection to improve patient's quality of life and general cognitive
9 functioning as well (third row in Table 1).

10
11 Despite these versatile possible implementations of DES, clinical trials of safety and
12 feasibility for improving memory and cognitive functioning have so far predominantly used
13 continuous chronic stimulation. One study employed DES in the fornix of the hippocampus
14 and tested the effect on various neuropsychological measures of declarative memory
15 functions in Alzheimer's disease patients⁹⁶⁻⁹⁸. Another study targeted nucleus basalis of
16 Meynert in Lewi body dementia^{99,100,101,102,99,100}. Although these trials resulted in interesting
17 observations like DES-induced flashbacks¹⁰³ or even significant improvements in single
18 cases¹⁰⁴, there were no consistent long-term effects on memory performance with that type
19 of stimulation. More consistent effects on cognitive functions were reported in other large
20 longitudinal studies of responsive stimulation. For instance, a study of long-term responsive
21 hippocampal stimulation for epilepsy treatment reported improved cognitive functioning
22 tested in neuropsychological assessments over multiple years of the DES therapy^{105,106}. In
23 this case, however, DES was targeted at the pathophysiological activities of epilepsy, hence
24 the effects on memory and cognition could have been a secondary indirect effect like in
25 another large study of continuous DES of the anterior nucleus of the thalamus^{107,108}. Safety
26 and efficacy of phasic stimulation types targeted specifically at the cognitive functions
27 remains to be demonstrated in pending clinical trials. Responsive DES driven by neural
28 biomarkers of electrophysiological activities holds promise for more robust and reproducible
29 results and more insight into the underlying neural mechanisms.

30
31 Even though it is possible to implement the various stimulation approaches into the non-
32 invasive methods (see Box 2), including the responsive stimulation, it is more challenging to
33 record and analyze the brain activities from the scalp EEG, MEG or vagus nerve signals. The

1 data quality of these signals in terms of the (1) signal-to-noise ratio, (2) ability to record from
2 deep brain regions, and (3) sensitivity to high-frequency signals) are superior with direct
3 techniques employing invasive electrodes. Furthermore, invasive DES is more powerful than
4 non-invasive tACS/TMS, especially in case of the deep brain targets where amplitude of the
5 non-invasive stimulation is strongly reduced with distance. There are also other, more
6 practical issues to consider like the recording equipment for sampling non-invasive signals,
7 which is not easily wearable outside of the experimental setup. Compared to fully
8 implantable invasive devices, the non-invasive scalp EEG electrodes or MEG magnets are
9 typically not adequate for applications beyond the laboratory setup. There are practical
10 limitations to using the non-invasive recording and stimulation methods for studying the
11 mechanisms and for modulation of memory functions acutely during experimentation and
12 chronically in everyday life performance.

13

14 **A new perspective for modulating memory and cognition**

15 The responsive DES studies for epilepsy management revealed an important insight into a
16 possible mechanism for improving memory and cognition. Patients' performance in cognitive
17 tasks was progressing together with the therapeutic effect of DES on epilepsy. Hence, the
18 positive effects on cognition could be achieved by alleviating the pathophysiological
19 activities of epilepsy and/or by modulation of physiological memory processes. Chronic
20 recordings from a recent study with repeatedly taken memory tasks showed clear correlations
21 between a gradually decreasing rate of seizures and a gradually improving task performance
22 in response to optimizing therapeutic parameters of DES ¹⁰⁹.

23

24 These results suggest a strategy to DES that is alternative to entrainment or to the attempts to
25 mimic a physiologically occurring activity pattern described above. Instead of improving or
26 boosting relatively physiological activities underlying memory processing, it may be more
27 promising to target pathological activities that interfere with cognitive functions or to
28 modulate malfunctioning memory processing. Restoration of memory functions may,
29 therefore, be due to alleviation in pathophysiology or due to stimulation-induced
30 counteraction of a detrimental brain state unrelated to any brain disorder. This logic is
31 congruent with an assumption that it is more feasible to restore a malfunctioning process than
32 to enhance a properly functioning one. It was found that DES is more likely to have a positive
33 effect when applied in a state of 'poor' than in a state of 'good' memory encoding as

1 predicted by iEEG spectral activities^{65,68}. In other words, DES can work more effectively by
2 tuning or rescuing suboptimal states of memory processing than by modulating or stabilizing
3 the ones that are already close to optimal. Either way, biomarkers of neural activities are
4 required in both strategies to trigger the timing, adjust the parameters, and/or change the
5 pattern of DES by monitoring its immediate and long-lasting effects. A good example is
6 provided with activities in the beta frequency range induced in the posterior brain regions by
7 non-invasive stimulation in the anterior prefrontal areas⁵⁷. The posterior beta activities
8 served as a biomarker of the positive effect, despite not necessarily reflecting the activities
9 underlying successful memory formation *per se*. Such biomarkers can be used over time to
10 assess and adjust DES for optimal performance.

11
12 This leads us to the concept of adaptive stimulation. It can be generally defined as intelligent
13 and flexible stimulation adjusted by biomarkers of neural activity. The main feature that
14 makes it different from the classic stimulation approaches summarized in Table 1 is the
15 ability to adapt over time, as the name implies, based on the history of biomarker analysis. It
16 is different to a classic implementation of responsive stimulation, which is driven by
17 biomarker analysis but is not adapted over time based on the history of outcomes. Therefore,
18 it can be regarded as a special case of responsive stimulation with adaptation of parameters
19 over time. One of its first applications was in the Deep Brain Stimulation (DBS) therapy for
20 Parkinson's disease^{110,111}. In this particular example, pathological oscillations in the beta
21 frequency range serve as the biomarker for modulating motor functions. Notice that here also
22 the stimulation is not targeting the healthy physiological processes of movement generation
23 to boost their underlying neural activities, but instead focuses on eliminating pathological
24 beta oscillations that possibly interfere with the physiological processing of movement
25 generation. In the original implementation of adaptive stimulation, the pathological beta
26 oscillations are detected in the recorded signal to inform the location and timing of
27 therapeutic DES. These can be adjusted online based on immediate local analysis or offline
28 based on long-term recordings streamed wirelessly from the implanted device. The former
29 (i.e., immediate local analysis as in¹¹²) could be conceived as a special case of responsive
30 stimulation, since the parameters are adjusted immediately on the implanted device; the latter
31 (i.e. long-term offline analysis as in¹⁰⁹) require integration to other computer devices or
32 cloud environments for more intensive analysis^{113,114} (Fig. 2), which enables adapting the
33 parameters based on a long history of stimulation outcomes that is too large to be stored on

1 the implanted device. Distributing data storage and analytics over to online resources opens
2 limitless opportunities for dense tracking and modulation of neural activities and behavior
3 ^{115,116}, as outcome measures to be compared across time. In Parkinson's patients ¹¹² and more
4 recently also in epilepsy ¹¹⁷, this biomarker-based approach provides arguably the first
5 'proof-of-concept' evidence of successful application of adaptive brain stimulation.
6

7 In terms of memory and cognition, such technology now enables chronic, real-life tracking of
8 a wide range of iEEG spectral activities that accompany memory processing and behavior ¹¹⁸⁻
9 ¹²¹. Compared to epilepsy or movement disorders, the target location and neural activities
10 during memory processing are more difficult to determine as they are dynamic in time and
11 distributed across the brain ^{119,122-124}. The spatiotemporal dynamics typically involve a wide
12 spectral frequency range of neural activities sampled from multiple implanted electrodes in
13 various brain regions, which requires intense automated multi-channel analyses of the
14 recorded signals. Particular electrode leads and activities thus have to be identified for DES
15 based on biomarkers of particular neural activities. Once established, these provide features
16 for fully automated machine-learning classification ¹²⁵, which can be run in a closed-loop on
17 distributed external devices or in virtual cloud environments (Fig. 2). Exploring the large
18 space of possible DES parameters to determine optimal settings can likewise be done by
19 automated computational methods ¹²⁶ based on desired biomarker outcomes (if known). In
20 this manner, the choice of particular electrode locations, parameters of the electrical current,
21 and DES timing has to be managed automatically using various intelligent data-driven tools
22 to efficiently find optimal solutions. Such algorithms would determine the optimal parameters
23 based on history of recordings and the effects on the biomarkers and behavior. Otherwise,
24 manually determining the parameters for modulation of cognitive processes becomes too
25 time-consuming and elusive, given their dynamic nature in time and anatomical space, and a
26 variety of underlying neural activities.
27

28 This flexible adjustment of the locations and parameters of DES to find optimal settings over
29 time is the defining feature for the concept of adaptive stimulation. The responsive
30 stimulation approach is fixed on a set of parameters without longitudinal assessment of the
31 outcome history of the stimulation settings. Adaptive stimulation compares the outcomes of
32 various DES parameters to find the optimal setting. Hence, in principle, it can employ other
33 types like non-responsive open-loop or even continuous DES, as long as the biomarker

1 outcomes of these are compared across the parameters sets . In its simplest form it can
2 employ continuous DES at particular parameter sets that are fixed for a period of time and
3 evaluated based on the history of recordings and offline manual expert analysis of biomarkers
4 without any automated biomarker analysis. This is very similar to the continuous approach
5 that is used for adjusting the DBS parameters for movement disorders or epilepsy during out-
6 patient hospital visits, but with the critical difference that in the classic DBS therapy the
7 parameter adjustment is made with no consideration of the long history of electrophysiologic
8 recordings. In this classic case, the adjustment is made predominantly based on the patient's
9 subjective report of symptoms and neurological exams. The defining feature of adaptive DBS
10 would be the consideration of the history of electrophysiological recordings and of
11 biomarkers such as epileptic discharges or pathological beta oscillations to guide the selection
12 of optimal parameters. Thus, adaptive stimulation is not a new type of DES but rather a more
13 general and flexible approach than the ones summarized in Table 1, which can employ any
14 combination of those to modulate brain functions.

15
16 Adaptive stimulation of the anterior nuclei of the thalamus (ANT) provides a pertinent case
17 study for chronic modulation of memory and possibly other cognitive functions related to
18 attention or mood ¹²⁷. This deep anatomical structure has become an attractive target
19 originally for epilepsy management ¹²⁸ and, more recently, also for modulating memory and
20 cognition ^{129–135}. It was shown that continuous stimulation of this structure leads to
21 improvements in memory task performance ⁹⁰. Longitudinal follow-up studies from a clinical
22 trial of continuous stimulation for epilepsy management reported beneficial effects on
23 cognitive functions assessed in periodic neuropsychological testing ^{107,108}. Hence, the anterior
24 thalamic nuclei became an attractive target to study and test the effects of DES in chronically
25 implanted patients. Repeated probing of memory performance and the underlying neural
26 activities with DES is now possible with the current technology at an unprecedented
27 timescale of months and years. Continuous recording of neural activities and simultaneous
28 assessment of behavioral performance revealed a strong effect of DES in ANT on
29 electrophysiological activity and verbal memory, i.e. significant changes in the theta power
30 and parallel improvements in the number of remembered words of up to 50% relative to the
31 baseline ^{109,136}. Specifically, a performance of approx. 4 remembered items was changed to an
32 average of 6 items in response to anterior thalamic stimulation (Fig. 3). Duration of this
33 improvement was observed on the scale of a year, as compared to a month reported in the
34 most recent study using non-invasive transcranial electrical stimulation ⁵⁹. This powerful

1 effect of adaptive ANT modulation correlated with (and was possibly driven by) reductions
2 in epilepsy pathophysiology as well as with modulation of physiological biomarkers of
3 anterior thalamic-hippocampal interactions that were induced by memory processing¹³⁶.
4 Such biomarkers are ideally suited for long-term adaptive DES targeting both epilepsy
5 pathophysiology as well as restoration of cognitive functions. In this particular example, a
6 moderate-to-severe deficit in recall of verbal memory was restored across almost 2 years of
7 stimulation to a normal performance, reaching almost the level typical for healthy
8 participants (Fig. 3). DES with electrical currents at low frequency (2-7Hz) proved more
9 effective in driving this effect over months of the adaptive stimulation therapy. The chronic
10 nature of this DES-driven improvement is a major advancement compared to the more short-
11 term effects of much lower magnitude reported in the previous studies.

12
13 This type of longitudinal recordings with adaptive optimization of stimulation based on
14 objective biomarkers presents exciting perspectives for treating and studying disorders of
15 memory and cognition. First of all, they are addressing basic research questions about the
16 approach to improving memory and cognitive performance: is it better to tune or entrain a
17 weak physiological process or activity that is about to fail, or rather to maintain and preserve
18 a strong one that is likely leading to a successful memory outcome^{61,65,67,68,79,80}?
19 Alternatively, one could specifically interfere with pathological activities, e.g., related to
20 epilepsy, that are detrimental to memory functions. Clinically, it is important to realize that
21 the stimulation parameters and the timing that are optimal for controlling disease, such as
22 epilepsy, may be different from optimal parameters for consolidating memory. This point
23 highlights the possibility of multilead devices targeting different brain circuits and processes
24 independently in order to optimally treat neurologic disease as well as associated
25 comorbidities.

26
27 Secondly, the longitudinal recordings with adaptive DES open avenues for Big Data analysis
28 of signals recorded continuously over months and years of daily lives. Supervised and
29 unsupervised machine-learning tools will be indispensable for mining and interpreting the
30 volumes of data that are already generated from the brains of implanted patients around the
31 world. Deep-learning is another tool that can potentially be applied to linear iEEG signals.
32 All this, in turn, will lead to development of new biomarkers and therapies that can be
33 flexibly adjusted over time by human experts supported by insights from machine-learning
34 tools. The entire process of adaptation could at some point be fully automated and driven

1 solely by biomarker analysis. For example, fading attention and memory functions, as
2 signaled by changes in biomarker features, would be automatically detected and trigger
3 administration of memory testing or a specific DES treatment. The treatment would be
4 determined from a large space of possible localization, timing and parameter options
5 competing for selection by optimization algorithms. This is a highly multidimensional space
6 that includes configurations of individual or multiple stimulating electrode(s) configurations,
7 current amplitude, frequency and patterns of stimulation like single-pulse, sine or square
8 waves or complex waveforms. The algorithms as well come in various types and flavors. In
9 other words, it would be a virtual *in silico* ‘survival of the fittest’ combination of parameters
10 automatically probed and selected by the algorithms based on the optimal output response
11 that can either be a change in memory performance or of an electrophysiological biomarker.
12

13 This analogy to the process of natural selection plays well with the concept of intelligent
14 adaptation of DES based on the history of data recordings and adjustment of hypothetical
15 future outcomes. With progress in neurotechnologies for probing and analyzing the neural
16 activities underlying memory and cognition, we will be entering into a new era of brain-
17 computer interfaces for neural engineering of the human mind ^{2,34,137}. It would be a point of
18 machine-learning literally encountering human learning at a neural interface. Such interfaces
19 would be qualitatively different from the current ones employed for movement or speech
20 generation, which arguably require skills that are already mostly learned and thus less
21 dynamic. The new interfaces for modulating dynamically changing memory processing will
22 need to adapt continuously over extended periods of time. This adaptation would need to
23 consider the changing brain states of wakefulness and sleep, and likely require continuous
24 tracking of slow wave sleep, which is now possible from single intracranial electrode contacts
25

138

27 **Conclusions**

28 In the last twenty years we have seen an emergence of invasive and non-invasive studies to
29 enhance memory performance. Most of them focused on acute effects of stimulation in
30 relatively small subject numbers in a limited timeframe, resulting in challenges for
31 consistency and reproducibility of the findings. Larger clinical trials employing continuous
32 stimulation over extended time periods yielded limited effects on long-term memory
33 performance. Despite impressive technological progress and a growing body of literature

1 showing positive effects of DES on memory and cognitive functions, our understanding of
2 the electrophysiological responses to stimulation tracked over extended periods of time is
3 limited, partly because of the lack of appropriate tools.

4
5 In addition to these challenges on a neurophysiological and technological level, it is still an
6 open question which patient populations may benefit the most from DES. Previous DES
7 studies were either conducted in presurgical epilepsy patients or in patients with more or less
8 advanced Alzheimer's disease. In AD patients, any interventions – be they based on DES or
9 pharmacological treatments – are most promising when applied in very early or even
10 preclinical disease stages. But then, conducting an invasive procedure in preclinical patients
11 is problematic in general and would require very reliable and specific predictors of disease
12 progression. The possibility of reversing advanced disease processes with brain stimulation is
13 more questionable and remains to be demonstrated in patients¹³⁹.

14
15 Nevertheless, important lessons have been learned about principled approaches to modulating
16 memory and cognition. There are multiple ways to stimulate the brain and modulate memory
17 performance. Targeting specific neural activities that support or interfere with memory
18 processing may be an effective strategy to achieve robust behavioral outcomes. Validating
19 biomarkers of these activities is key to monitoring and optimizing new responsive DES
20 approaches chronically. This is proving particularly useful for the new implantable
21 technologies for chronic recording and stimulation. Adaptive DES emerges as an attractive
22 approach for tracking and modulating the highly dynamic processes of memory formation.
23 Chronic intelligent adaptation of DES based on personalized biomarker-driven analysis
24 promises to deliver powerful and lasting therapeutic effects in not only neurological but also
25 neuropsychiatric brain disorders^{140, 141,142}.

26
27 We foresee that the new chronic biomarker approach to adaptive DES will drive further
28 development in technologies for high-density multi-channel recordings that are capable of
29 sampling large-scale electrophysiological activities, ranging from action potentials of
30 neuronal assemblies to network oscillations across widespread neural populations. These
31 technologies will inevitably produce large volumes of data that require automated machine-
32 learning tools distributed over local and remote processing environments. The technological
33 development will, in turn, open new opportunities for extending the loop of data analysis for
34 responsive brain stimulation to the virtual environments of internet and cloud computations.

1 It presents unprecedented advantages and possibilities for modulation and interfacing with
2 memory and the associated cognitive processes of the human mind. The ensuing neuroethical
3 issues are already becoming a challenge to the ‘brave new world’ of DES for modulating
4 human declarative memory.

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13 **Competing interests**

14 The authors report no competing interests.

15 **References**

- 16 1. Squire LR, Zola SM. Structure and function of declarative and nondeclarative memory
17 systems. *Proc Natl Acad Sci U S A*. 1996;93(24):13515-13522.
- 18 2. Johnson EL, Kam JWY, Tzovara A, Knight RT. Insights into human cognition from
19 intracranial EEG: A review of audition, memory, internal cognition, and causality. *J Neural Eng*.
20 2020;17(5):051001.
- 21 3. Johnson EL, Knight RT. Intracranial recordings and human memory. *Current Opinion in*
22 *Neurobiology*. 2015;31:18-25. doi:10.1016/j.conb.2014.07.021
- 23 4. Mukamel R, Fried I. Human intracranial recordings and cognitive neuroscience. *Annu Rev*
24 *Psychol*. 2012;63:511-537.
- 25 5. Fried I, Rutishauser U, Cerf M, Kreiman G. *Single Neuron Studies of the Human Brain:*
26 *Probing Cognition*. MIT Press; 2014.
- 27 6. Jacobs J, Kahana MJ. Direct brain recordings fuel advances in cognitive electrophysiology.
28 *Trends Cogn Sci*. 2010;14(4):162-171.

- 1 7. Huijbers W, Vannini P, Sperling RA, C M P, Cabeza R, Daselaar SM. Explaining the
2 encoding/retrieval flip: memory-related deactivations and activations in the posteromedial cortex.
3 *Neuropsychologia*. 2012;50(14):3764-3774.
- 4 8. Linde-Domingo J, Treder MS, Kerrén C, Wimber M. Evidence that neural information flow is
5 reversed between object perception and object reconstruction from memory. *Nat Commun*.
6 2019;10(1):179.
- 7 9. Hasselmo ME, Bodelón C, Wyble BP. A proposed function for hippocampal theta rhythm:
8 separate phases of encoding and retrieval enhance reversal of prior learning. *Neural Comput*.
9 2002;14(4):793-817.
- 10 10. Allan K, Allen R. Retrieval attempts transiently interfere with concurrent encoding of
11 episodic memories but not vice versa. *J Neurosci*. 2005;25(36):8122-8130.
- 12 11. Xue G. The Neural Representations Underlying Human Episodic Memory. *Trends Cogn Sci*.
13 2018;22(6):544-561.
- 14 12. Dudai Y, Karni A, Born J. The Consolidation and Transformation of Memory. *Neuron*.
15 2015;88(1):20-32.
- 16 13. Anderson MC, Green C. Suppressing unwanted memories by executive control. *Nature*.
17 2001;410(6826):366-369.
- 18 14. Engen HG, Anderson MC. Memory Control: A Fundamental Mechanism of Emotion
19 Regulation. *Trends Cogn Sci*. 2018;22(11):982-995.
- 20 15. Penfield W, Perot P. THE BRAIN'S RECORD OF AUDITORY AND VISUAL
21 EXPERIENCE. A FINAL SUMMARY AND DISCUSSION. *Brain*. 1963;86:595-696.
- 22 16. Penfield W. SOME MECHANISMS OF CONSCIOUSNESS DISCOVERED DURING
23 ELECTRICAL STIMULATION OF THE BRAIN. *Proc Natl Acad Sci U S A*. 1958;44(2):51-66.
- 24 17. Fox KCR, Shi L, Baek S, et al. Intrinsic network architecture predicts the effects elicited by
25 intracranial electrical stimulation of the human brain. *Nature Human Behaviour*. 2020;4(10):1039-
26 1052. doi:10.1038/s41562-020-0910-1
- 27 18. Histed MH, Bonin V, Reid RC. Direct activation of sparse, distributed populations of cortical
28 neurons by electrical microstimulation. *Neuron*. 2009;63(4):508-522.
- 29 19. Mohan UR, Watrous AJ, Miller JF, et al. The effects of direct brain stimulation in humans
30 depend on frequency, amplitude, and white-matter proximity. *Brain Stimul*. 2020;13(5):1183-1195.
- 31 20. Solomon EA, Kragel JE, Gross R, et al. Medial temporal lobe functional connectivity predicts
32 stimulation-induced theta power. *Nat Commun*. 2018;9(1):4437.
- 33 21. Solomon EA, Sperling MR, Sharan AD, et al. Theta-burst stimulation entrains frequency-
34 specific oscillatory responses. *Brain Stimul*. 2021;14(5):1271-1284.
- 35 22. Lech M, Berry B, Topcu C, et al. Direct Electrical Stimulation of the Human Brain Has
36 Inverse Effects on the Theta and Gamma Neural Activities. *IEEE Trans Biomed Eng*.
37 2021;68(12):3701-3712.
- 38 23. Mankin EA, Aghajian ZM, Schuette P, et al. Stimulation of the right entorhinal white matter
39 enhances visual memory encoding in humans. *Brain Stimul*. 2021;14(1):131-140.
- 40 24. Kucewicz MT, Berry BM, Miller LR, et al. Evidence for verbal memory enhancement with

- 1 electrical brain stimulation in the lateral temporal cortex. *Brain*. 2018;141(4):971-978.
- 2 25. Ezzyat Y, Wanda PA, Levy DF, et al. Closed-loop stimulation of temporal cortex rescues
3 functional networks and improves memory. *Nat Commun*. 2018;9(1):365.
- 4 26. Borchers S, Himmelbach M, Logothetis N, Karnath HO. Direct electrical stimulation of
5 human cortex - the gold standard for mapping brain functions? *Nat Rev Neurosci*. 2011;13(1):63-70.
- 6 27. Moheimanian L, Paraskevopoulou SE, Adamek M, Schalk G, Brunner P. Modulation in
7 cortical excitability disrupts information transfer in perceptual-level stimulus processing. *Neuroimage*.
8 2021;243:118498.
- 9 28. Lakatos P, Shah AS, Knuth KH, Ulbert I, Karmos G, Schroeder CE. An oscillatory hierarchy
10 controlling neuronal excitability and stimulus processing in the auditory cortex. *J Neurophysiol*.
11 2005;94(3):1904-1911.
- 12 29. Helfrich RF, Fiebelkorn IC, Szczepanski SM, et al. Neural Mechanisms of Sustained
13 Attention Are Rhythmic. *Neuron*. 2018;99(4):854-865.e5.
- 14 30. Fusi S, Miller EK, Rigotti M. Why neurons mix: high dimensionality for higher cognition.
15 *Curr Opin Neurobiol*. 2016;37:66-74.
- 16 31. Suthana N, Haneef Z, Stern J, et al. Memory enhancement and deep-brain stimulation of the
17 entorhinal area. *N Engl J Med*. 2012;366(6):502-510.
- 18 32. Jacobs J, Miller J, Lee SA, et al. Direct Electrical Stimulation of the Human Entorhinal
19 Region and Hippocampus Impairs Memory. *Neuron*. 2016;92(5):983-990.
- 20 33. Titiz AS, Hill MRH, Mankin EA, et al. Theta-burst microstimulation in the human entorhinal
21 area improves memory specificity. *Elife*. 2017;6. doi:10.7554/eLife.29515
- 22 34. Mankin EA, Fried I. Modulation of Human Memory by Deep Brain Stimulation of the
23 Entorhinal-Hippocampal Circuitry. *Neuron*. 2020;106(2):218-235.
- 24 35. Suthana N, Aghajan ZM, Mankin EA, Lin A. Reporting Guidelines and Issues to Consider for
25 Using Intracranial Brain Stimulation in Studies of Human Declarative Memory. *Front Neurosci*.
26 2018;12:905.
- 27 36. Kim K, Ekstrom AD, Tandon N. A network approach for modulating memory processes via
28 direct and indirect brain stimulation: Toward a causal approach for the neural basis of memory.
29 *Neurobiol Learn Mem*. 2016;134 Pt A:162-177.
- 30 37. Jacobs J, Lega B, Anderson C. Explaining how brain stimulation can evoke memories. *J*
31 *Cogn Neurosci*. 2012;24(3):553-563.
- 32 38. Hamani C, McAndrews MP, Cohn M, et al. Memory enhancement induced by
33 hypothalamic/fornix deep brain stimulation. *Ann Neurol*. 2008;63(1):119-123.
- 34 39. McLachlan RS, Pigott S, Tellez-Zenteno JF, Wiebe S, Parrent A. Bilateral hippocampal
35 stimulation for intractable temporal lobe epilepsy: impact on seizures and memory. *Epilepsia*.
36 2010;51(2):304-307.
- 37 40. Koubeissi MZ, Kahrman E, Syed TU, Miller J, Durand DM. Low-frequency electrical
38 stimulation of a fiber tract in temporal lobe epilepsy. *Ann Neurol*. 2013;74(2):223-231.
- 39 41. Coleshill SG, Binnie CD, Morris RG, et al. Material-specific recognition memory deficits
40 elicited by unilateral hippocampal electrical stimulation. *J Neurosci*. 2004;24(7):1612-1616.

- 1 42. Fell J, Staresina BP, Do Lam ATA, et al. Memory modulation by weak synchronous deep
2 brain stimulation: a pilot study. *Brain Stimul.* 2013;6(3):270-273.
- 3 43. Miller JP, Sweet JA, Bailey CM, Munyon CN, Luders HO, Fastenau PS. Visual-spatial
4 memory may be enhanced with theta burst deep brain stimulation of the fornix: a preliminary
5 investigation with four cases. *Brain.* 2015;138(Pt 7):1833-1842.
- 6 44. Laxton AW, Tang-Wai DF, McAndrews MP, et al. A phase I trial of deep brain stimulation of
7 memory circuits in Alzheimer's disease. *Ann Neurol.* 2010;68(4):521-534.
- 8 45. Boëx C, Seeck M, Vulliémoz S, et al. Chronic deep brain stimulation in mesial temporal lobe
9 epilepsy. *Seizure.* 2011;20(6):485-490.
- 10 46. Miatton M, Van Roost D, Thiery E, et al. The cognitive effects of amygdalohippocampal
11 deep brain stimulation in patients with temporal lobe epilepsy. *Epilepsy Behav.* 2011;22(4):759-764.
- 12 47. Velasco AL, Velasco F, Velasco M, Trejo D, Castro G, Carrillo-Ruiz JD. Electrical
13 stimulation of the hippocampal epileptic foci for seizure control: a double-blind, long-term follow-up
14 study. *Epilepsia.* 2007;48(10):1895-1903.
- 15 48. Lacruz ME, Valentín A, Seoane JJG, Morris RG, Selway RP, Alarcón G. Single pulse
16 electrical stimulation of the hippocampus is sufficient to impair human episodic memory.
17 *Neuroscience.* 2010;170(2):623-632.
- 18 49. Halgren E, Wilson CL, Stapleton JM. Human medial temporal-lobe stimulation disrupts both
19 formation and retrieval of recent memories. *Brain Cogn.* 1985;4(3):287-295.
- 20 50. Perrine K, Devinsky O, Uysal S, Luciano DJ, Dogali M. Left temporal neocortex mediation
21 of verbal memory: evidence from functional mapping with cortical stimulation. *Neurology.*
22 1994;44(10):1845-1850.
- 23 51. Jun S, Kim JS, Chung CK. Direct Stimulation of Human Hippocampus During Verbal
24 Associative Encoding Enhances Subsequent Memory Recollection. *Frontiers in Human*
25 *Neuroscience.* 2019;13. doi:10.3389/fnhum.2019.00023
- 26 52. Antal A, Luber B, Brem AK, et al. Non-invasive brain stimulation and neuroenhancement.
27 *Clin Neurophysiol Pract.* 2022;7:146-165.
- 28 53. Begemann MJ, Brand BA, Ćurčić-Blake B, Aleman A, Sommer IE. Efficacy of non-invasive
29 brain stimulation on cognitive functioning in brain disorders: a meta-analysis. *Psychol Med.*
30 2020;50(15):2465-2486.
- 31 54. Phipps CJ, Murman DL, Warren DE. Stimulating Memory: Reviewing Interventions Using
32 Repetitive Transcranial Magnetic Stimulation to Enhance or Restore Memory Abilities. *Brain Sci.*
33 2021;11(10). doi:10.3390/brainsci11101283
- 34 55. Goldthorpe RA, Rapley JM, Violante IR. A Systematic Review of Non-invasive Brain
35 Stimulation Applications to Memory in Healthy Aging. *Front Neurol.* 2020;11:575075.
- 36 56. Rosenblum Y, Dresler M. Can brain stimulation boost memory performance? *PLoS Biol.*
37 2021;19(9):e3001404.
- 38 57. van der Plas M, Braun V, Stauch BJ, Hanslmayr S. Stimulation of the left dorsolateral
39 prefrontal cortex with slow rTMS enhances verbal memory formation. *PLoS Biol.*
40 2021;19(9):e3001363.
- 41 58. O'Leary K. Brain stimulation boosts memory in older adults. *Nat Med.* Published online

- 1 August 31, 2022. doi:10.1038/d41591-022-00089-x
- 2 59. Grover S, Wen W, Viswanathan V, Gill CT, Reinhart RMG. Long-lasting, dissociable
3 improvements in working memory and long-term memory in older adults with repetitive
4 neuromodulation. *Nat Neurosci*. Published online August 22, 2022. doi:10.1038/s41593-022-01132-3
- 5 60. Wang JX, Rogers LM, Gross EZ, et al. Targeted enhancement of cortical-hippocampal brain
6 networks and associative memory. *Science*. 2014;345(6200):1054-1057.
- 7 61. Hanslmayr S, Axmacher N, Inman CS. Modulating Human Memory via Entrainment of Brain
8 Oscillations. *Trends Neurosci*. 2019;42(7):485-499.
- 9 62. Sarica C, Nankoo JF, Fomenko A, et al. Human Studies of Transcranial Ultrasound
10 neuromodulation: A systematic review of effectiveness and safety. *Brain Stimul*. 2022;15(3):737-746.
- 11 63. Legon W, Sato TF, Opitz A, et al. Transcranial focused ultrasound modulates the activity of
12 primary somatosensory cortex in humans. *Nat Neurosci*. 2014;17(2):322-329.
- 13 64. Beisteiner R, Matt E, Fan C, et al. Transcranial pulse stimulation with ultrasound in
14 Alzheimer's disease—A new navigated focal brain therapy. *Adv Sci*. 2020;7(3):1902583.
- 15 65. Kucewicz MT, Berry BM, Kremen V, et al. Electrical Stimulation Modulates High γ Activity
16 and Human Memory Performance. *eNeuro*. 2018;5(1). doi:10.1523/ENEURO.0369-17.2018
- 17 66. Goyal A, Miller J, Watrous AJ, et al. Electrical Stimulation in Hippocampus and Entorhinal
18 Cortex Impairs Spatial and Temporal Memory. *J Neurosci*. 2018;38(19):4471-4481.
- 19 67. Ezzyat Y, Rizzuto DS. Direct brain stimulation during episodic memory. *Current Opinion in*
20 *Biomedical Engineering*. 2018;8:78-83. doi:10.1016/j.cobme.2018.11.004
- 21 68. Ezzyat Y, Kragel JE, Burke JF, et al. Direct Brain Stimulation Modulates Encoding States
22 and Memory Performance in Humans. *Curr Biol*. 2017;27(9):1251-1258.
- 23 69. Saboo KV, Varatharajah Y, Berry BM, et al. A Computationally Efficient Model for
24 Predicting Successful Memory Encoding Using Machine-Learning-based EEG Channel Selection.
25 *2019 9th International IEEE/EMBS Conference on Neural Engineering (NER)*. Published online
26 2019. doi:10.1109/ner.2019.8717057
- 27 70. Jun S, Lee SA, Kim JS, Jeong W, Chung CK. Task-dependent effects of intracranial
28 hippocampal stimulation on human memory and hippocampal theta power. *Brain Stimul*.
29 2020;13(3):603-613.
- 30 71. Inman CS, Manns JR, Bijanki KR, et al. Direct electrical stimulation of the amygdala
31 enhances declarative memory in humans. *Proc Natl Acad Sci U S A*. 2018;115(1):98-103.
- 32 72. Fell J, Klaver P, Lehnertz K, et al. Human memory formation is accompanied by rhinal-
33 hippocampal coupling and decoupling. *Nat Neurosci*. 2001;4(12):1259-1264.
- 34 73. Alagapan S, Riddle J, Huang WA, Hadar E, Shin HW, Fröhlich F. Network-Targeted, Multi-
35 site Direct Cortical Stimulation Enhances Working Memory by Modulating Phase Lag of Low-
36 Frequency Oscillations. *Cell Rep*. 2019;29(9):2590-2598.e4.
- 37 74. Alagapan S, Lustenberger C, Hadar E, Shin HW, Fröhlich F. Low-frequency direct cortical
38 stimulation of left superior frontal gyrus enhances working memory performance. *Neuroimage*.
39 2019;184:697-706.
- 40 75. Hampson RE, Song D, Robinson BS, et al. Developing a hippocampal neural prosthetic to

- 1 facilitate human memory encoding and recall. *J Neural Eng.* 2018;15(3):036014.
- 2 76. Sendi MSE, Inman CS, Bijanki KR, et al. Identifying the neurophysiological effects of
3 memory-enhancing amygdala stimulation using interpretable machine learning. *Brain Stimul.*
4 2021;14(6):1511-1519.
- 5 77. Hansen N, Chaieb L, Derner M, et al. Memory encoding-related anterior hippocampal
6 potentials are modulated by deep brain stimulation of the entorhinal area. *Hippocampus.*
7 2018;28(1):12-17.
- 8 78. Burke JF, Merkow MB, Jacobs J, Kahana MJ, Zaghoul KA. Brain computer interface to
9 enhance episodic memory in human participants. *Front Hum Neurosci.* 2014;8:1055.
- 10 79. Sreekumar V, Wittig JH Jr, Sheehan TC, Zaghoul KA. Principled Approaches to Direct
11 Brain Stimulation for Cognitive Enhancement. *Front Neurosci.* 2017;11:650.
- 12 80. Lee H, Fell J, Axmacher N. Electrical engram: how deep brain stimulation affects memory.
13 *Trends Cogn Sci.* 2013;17(11):574-584.
- 14 81. Amengual JL, Vernet M, Adam C, Valero-Cabré A. Local entrainment of oscillatory activity
15 induced by direct brain stimulation in humans. *Sci Rep.* 2017;7:41908.
- 16 82. Herrington TM, Cheng JJ, Eskandar EN. Mechanisms of deep brain stimulation. *J*
17 *Neurophysiol.* 2016;115(1):19-38.
- 18 83. Montgomery EB Jr, Gale JT. Mechanisms of action of deep brain stimulation(DBS). *Neurosci*
19 *Biobehav Rev.* 2008;32(3):388-407.
- 20 84. McIntyre CC, Savasta M, Walter BL, Vitek JL. How does deep brain stimulation work?
21 Present understanding and future questions. *J Clin Neurophysiol.* 2004;21(1):40-50.
- 22 85. Johnson MD, Miocinovic S, McIntyre CC, Vitek JL. Mechanisms and targets of deep brain
23 stimulation in movement disorders. *Neurotherapeutics.* 2008;5(2):294-308.
- 24 86. Ashkan K, Rogers P, Bergman H, Ughratdar I. Insights into the mechanisms of deep brain
25 stimulation. *Nat Rev Neurol.* 2017;13(9):548-554.
- 26 87. Jakobs M, Fomenko A, Lozano AM, Kiening KL. Cellular, molecular, and clinical
27 mechanisms of action of deep brain stimulation-a systematic review on established indications and
28 outlook on future developments. *EMBO Mol Med.* 2019;11(4). doi:10.15252/emmm.201809575
- 29 88. Khan IS, D'Agostino EN, Calnan DR, Lee JE, Aronson JP. Deep Brain Stimulation for
30 Memory Modulation: A New Frontier. *World Neurosurg.* 2019;126:638-646.
- 31 89. Tan SZK, Fung ML, Koh J, Chan YS, Lim LW. The Paradoxical Effect of Deep Brain
32 Stimulation on Memory. *Aging Dis.* 2020;11(1):179-190.
- 33 90. Oh YS, Kim HJ, Lee KJ, Kim YI, Lim SC, Shon YM. Cognitive improvement after long-term
34 electrical stimulation of bilateral anterior thalamic nucleus in refractory epilepsy patients. *Seizure.*
35 2012;21(3):183-187.
- 36 91. Chiang S, Rao V, Worrell G, Baud MO. *Seizure Forecasting and Detection: Computational*
37 *Models, Machine Learning, and Translation into Devices.* Frontiers Media SA; 2022.
- 38 92. Schelter B, Feldwisch-Drentrup H, Ihle M, Schulze-Bonhage A, Timmer J. Seizure prediction
39 in epilepsy: From circadian concepts via probabilistic forecasting to statistical evaluation. 2011
40 *Annual International Conference of the IEEE Engineering in Medicine and Biology Society.*

- 1 Published online 2011. doi:10.1109/iembs.2011.6090469
- 2 93. Gregg NM, Sladky V, Nejedly P, et al. Thalamic deep brain stimulation modulates cycles of
3 seizure risk in epilepsy. *Sci Rep.* 2021;11(1):24250.
- 4 94. Gregg NM, Nasser M, Kremen V, et al. Circadian and multiday seizure periodicities, and
5 seizure clusters in canine epilepsy. *Brain Commun.* 2020;2(1):fcaa008.
- 6 95. Baud MO, Kleen JK, Mirro EA, et al. Multi-day rhythms modulate seizure risk in epilepsy.
7 *Nat Commun.* 2018;9(1):88.
- 8 96. Leoutsakos JMS, Yan H, Anderson WS, et al. Deep Brain Stimulation Targeting the Fornix
9 for Mild Alzheimer Dementia (the ADvance Trial): A Two Year Follow-up Including Results of
10 Delayed Activation. *J Alzheimers Dis.* 2018;64(2):597-606.
- 11 97. Lozano AM, Fosdick L, Chakravarty MM, et al. A Phase II Study of Fornix Deep Brain
12 Stimulation in Mild Alzheimer's Disease. *J Alzheimers Dis.* 2016;54(2):777-787.
- 13 98. Laxton AW, Tang-Wai DF, McAndrews MP, et al. A phase I trial of deep brain stimulation of
14 memory circuits in Alzheimer's disease. *Ann Neurol.* 2010;68(4):521-534.
- 15 99. Maltête D, Wallon D, Bourilhon J, et al. Nucleus Basalis of Meynert Stimulation for Lewy
16 Body Dementia. *Neurology.* 2021;96(5):e684-e697. doi:10.1212/wnl.0000000000011227
- 17 100. Liu W, Yu DY. Bilateral nucleus basalis of Meynert deep brain stimulation for dementia with
18 Lewy bodies: A randomised clinical trial. *Brain Stimulation.* 2020;13(6):1612-1613.
19 doi:10.1016/j.brs.2020.09.020
- 20 101. Kuhn J, Hardenacke K, Shubina E, et al. Deep Brain Stimulation of the Nucleus Basalis of
21 Meynert in Early Stage of Alzheimer's Dementia. *Brain Stimul.* 2015;8(4):838-839.
- 22 102. Kuhn J, Hardenacke K, Lenartz D, et al. Deep brain stimulation of the nucleus basalis of
23 Meynert in Alzheimer's dementia. *Mol Psychiatry.* 2015;20(3):353-360.
- 24 103. Deeb W, Salvato B, Almeida L, et al. Fornix-Region Deep Brain Stimulation-Induced
25 Memory Flashbacks in Alzheimer's Disease. *N Engl J Med.* 2019;381(8):783-785.
- 26 104. Zhang W, Liu W, Patel B, et al. Case Report: Deep Brain Stimulation of the Nucleus Basalis
27 of Meynert for Advanced Alzheimer's Disease. *Front Hum Neurosci.* 2021;15:645584.
- 28 105. Bergey GK, Morrell MJ, Mizrahi EM, et al. Long-term treatment with responsive brain
29 stimulation in adults with refractory partial seizures. *Neurology.* 2015;84(8):810-817.
- 30 106. Nair DR, Laxer KD, Weber PB, et al. Nine-year prospective efficacy and safety of brain-
31 responsive neurostimulation for focal epilepsy. *Neurology.* 2020;95(9):e1244-e1256.
- 32 107. Tröster AI, Meador KJ, Irwin CP, Fisher RS, SANTE Study Group. Memory and mood
33 outcomes after anterior thalamic stimulation for refractory partial epilepsy. *Seizure.* 2017;45:133-141.
- 34 108. King-Stephens D. Cheers for SANTÉ: Long Term Safety and Efficacy of Anterior Nucleus of
35 the Thalamus DBS. *Epilepsy Currents.* 2021;21(5):334-336. doi:10.1177/15357597211029169
- 36 109. Marks VS, Richner TJ, Gregg NM, et al. Deep Brain Stimulation of Anterior Nuclei of the
37 Thalamus and Hippocampal Seizure Rate Modulate Verbal Memory Performance. *2022 IEEE*
38 *International Conference on Electro Information Technology (eIT).* Published online 2022.
39 doi:10.1109/eit53891.2022.9813930

- 1 110. Little S, Pogosyan A, Neal S, et al. Adaptive deep brain stimulation in advanced Parkinson
2 disease. *Ann Neurol.* 2013;74(3):449-457.
- 3 111. Oyama G, Bovet A, Kamo H, et al. Adaptive deep brain stimulation in real world: First
4 observational data from the Japanese Early Adapter studies on adaptive deep brain stimulation
5 (aDBS). *Brain Stimulation.* 2021;14(6):1600-1601. doi:10.1016/j.brs.2021.10.041
- 6 112. Gilron R 'ee, Little S, Perrone R, et al. Long-term wireless streaming of neural recordings for
7 circuit discovery and adaptive stimulation in individuals with Parkinson's disease. *Nat Biotechnol.*
8 2021;39(9):1078-1085.
- 9 113. Sladky V, Nejedly P, Mivalt F, et al. Distributed brain co-processor for tracking
10 electrophysiology and behavior during electrical brain stimulation. doi:10.1101/2021.03.08.434476
- 11 114. Kremen V, Brinkmann BH, Kim I, et al. Integrating Brain Implants With Local and
12 Distributed Computing Devices: A Next Generation Epilepsy Management System. *IEEE J Transl*
13 *Eng Health Med.* 2018;6:2500112.
- 14 115. Mivalt F, Kremen V, Sladky V, et al. Electrical Brain Stimulation and Continuous Behavioral
15 State Tracking in Ambulatory Humans. doi:10.1101/2021.08.10.21261645
- 16 116. Attia TP, Crepeau D, Kremen V, et al. Epilepsy Personal Assistant Device—A Mobile
17 Platform for Brain State, Dense Behavioral and Physiology Tracking and Controlling Adaptive
18 Stimulation. *Frontiers in Neurology.* 2021;12. doi:10.3389/fneur.2021.704170
- 19 117. Sladky, Gregg, Mivalt, Marks. Hippocampal-ANT connectivity and ANT DBS: Circadian
20 trends and response to stimulation. *Clin Res Cardiol.* [https://www.brainstimjrn.com/article/S1935-](https://www.brainstimjrn.com/article/S1935-861X(21)00455-1/abstract)
21 [861X\(21\)00455-1/abstract](https://www.brainstimjrn.com/article/S1935-861X(21)00455-1/abstract)
- 22 118. Burke JF, Zaghoul KA, Jacobs J, et al. Synchronous and asynchronous theta and gamma
23 activity during episodic memory formation. *J Neurosci.* 2013;33(1):292-304.
- 24 119. Marks VS, Saboo KV, Topçu Ç, et al. Independent dynamics of low, intermediate, and high
25 frequency spectral intracranial EEG activities during human memory formation. *Neuroimage.*
26 2021;245:118637.
- 27 120. Kucewicz MT, Cimbalnik J, Matsumoto JY, et al. High frequency oscillations are associated
28 with cognitive processing in human recognition memory. *Brain.* 2014;137(Pt 8):2231-2244.
- 29 121. Fell J, Ludowig E, Staresina BP, et al. Medial temporal theta/alpha power enhancement
30 precedes successful memory encoding: evidence based on intracranial EEG. *J Neurosci.*
31 2011;31(14):5392-5397.
- 32 122. Kucewicz MT, Saboo K, Berry BM, et al. Human Verbal Memory Encoding Is Hierarchically
33 Distributed in a Continuous Processing Stream. *eNeuro.* 2019;6(1). doi:10.1523/ENEURO.0214-
34 18.2018
- 35 123. Zhang H, Watrous AJ, Patel A, Jacobs J. Theta and Alpha Oscillations Are Traveling Waves
36 in the Human Neocortex. *Neuron.* 2018;98(6):1269-1281.e4.
- 37 124. Burke JF, Long NM, Zaghoul KA, Sharan AD, Sperling MR, Kahana MJ. Human
38 intracranial high-frequency activity maps episodic memory formation in space and time. *Neuroimage.*
39 2014;85 Pt 2:834-843.
- 40 125. Saboo KV, Varatharajah Y, Berry BM, et al. Unsupervised machine-learning classification of
41 electrophysiologically active electrodes during human cognitive task performance. *Sci Rep.*
42 2019;9(1):17390.

- 1 126. Stieve BJ, Richner TJ, Krook-Magnuson C, Netoff TI, Krook-Magnuson E. Optimization of
2 closed-loop electrical stimulation enables robust cerebellar-directed seizure control. *Brain*. Published
3 online February 8, 2022. doi:10.1093/brain/awac051
- 4 127. Sun L, Peräkylä J, Polvivaara M, et al. Human anterior thalamic nuclei are involved in
5 emotion–attention interaction. *Neuropsychologia*. 2015;78:88-94.
- 6 128. Child ND, Benarroch EE. Anterior nucleus of the thalamus: Functional organization and
7 clinical implications. *Neurology*. 2013;81(21):1869-1876. doi:10.1212/01.wnl.0000436078.95856.56
- 8 129. Nelson AJD. The anterior thalamic nuclei and cognition: A role beyond space? *Neurosci*
9 *Biobehav Rev*. 2021;126:1-11.
- 10 130. Leszczyński M, Staudigl T. Memory-guided attention in the anterior thalamus. *Neurosci*
11 *Biobehav Rev*. 2016;66:163-165.
- 12 131. Sweeney-Reed CM, Buentjen L, Voges J, et al. The role of the anterior nuclei of the thalamus
13 in human memory processing. *Neurosci Biobehav Rev*. 2021;126:146-158.
- 14 132. Štillová K, Jurák P, Chládek J, et al. The Role of Anterior Nuclei of the Thalamus: A
15 Subcortical Gate in Memory Processing: An Intracerebral Recording Study. *PLoS One*.
16 2015;10(11):e0140778.
- 17 133. Liu J, Yu T, Wu J, et al. Anterior thalamic stimulation improves working memory precision
18 judgments. *Brain Stimul*. 2021;14(5):1073-1080.
- 19 134. Roy DS, Zhang Y, Aida T, et al. Anterior thalamic circuits crucial for working memory. *Proc*
20 *Natl Acad Sci U S A*. 2022;119(20):e2118712119.
- 21 135. Sweeney-Reed CM, Zaehle T, Voges J, et al. Pre-stimulus thalamic theta power predicts
22 human memory formation. *Neuroimage*. 2016;138:100-108.
- 23 136. Marks VS, Lech M, Gregg NM, et al. Chronic modulation of human memory and thalamic-
24 hippocampal theta activities. *In Review (preprint)*. Published online 2022.
- 25 137. Roelfsema PR, Denys D, Klink PC. Mind Reading and Writing: The Future of
26 Neurotechnology. *Trends Cogn Sci*. 2018;22(7):598-610.
- 27 138. Kremen V, Brinkmann BH, Van Gompel JJ, Stead M, St Louis EK, Worrell GA. Automated
28 unsupervised behavioral state classification using intracranial electrophysiology. *J Neural Eng*.
29 2019;16(2):026004.
- 30 139. McDermott B, Porter E, Hughes D, et al. Gamma Band Neural Stimulation in Humans and
31 the Promise of a New Modality to Prevent and Treat Alzheimer’s Disease. *J Alzheimers Dis*.
32 2018;65(2):363-392.
- 33 140. Bina RW, Langevin JP. Closed Loop Deep Brain Stimulation for PTSD, Addiction, and
34 Disorders of Affective Facial Interpretation: Review and Discussion of Potential Biomarkers and
35 Stimulation Paradigms. *Front Neurosci*. 2018;12:300.
- 36 141. Scangos KW, Makhoul GS, Sugrue LP, Chang EF, Krystal AD. State-dependent responses to
37 intracranial brain stimulation in a patient with depression. *Nat Med*. 2021;27(2):229-231.
- 38 142. Figeo M, Mayberg H. The future of personalized brain stimulation. *Nature Medicine*.
39 2021;27(2):196-197. doi:10.1038/s41591-021-01243-7

1 **Figure legends**

2 **Figure 1 Summary of key findings from the Restoring Active Memory multi-site**
3 **collaborative project (RAM).** First of all, the project failed to replicate the positive effects
4 of DES in mesial temporal lobe structures and found that stimulation in this region in many
5 cases actually impairs verbal and spatial memory. Second, DES applied during predicted poor
6 memory states had a beneficial effect on memory. The beneficial effect was selective to
7 stimulation in the lateral temporal cortex. Third, responsive (closed-loop) DES in that brain
8 region during poor memory states resulted in the same magnitude of memory enhancement
9 (approx. 15%) as non-responsive (open-loop) stimulation. Adapted from Jacobs et al. 2016,
10 Ezzayat et al. 2017 & 2018, and Kucewicz et al. 2018.

11
12 **Figure 2 Example of adaptive DES based on continuous recording and data analysis**
13 **distributed in closed loops of feedback response.** Schematic diagram of possible scenarios
14 for responsive stimulation in three closed loops of gradually more distributed and
15 externalized brain-computer interface settings (left). Example of a closed-loop extension of
16 data processing from an implanted device to distributed co-processing on external computer
17 and cloud analytics of electrophysiological biomarkers (right). In this particular example,
18 epileptic activities are automatically detected with machine-learning tools in the iEEG
19 recordings streamed for cloud analytics. This provides biomarkers for adjusting the brain
20 stimulation therapy for epilepsy and its comorbidities, including deficits in memory,
21 cognition and mood. Adapted from Sladky et. al 2022.

22
23 **Figure 3 Long-term adaptive modulation of memory performance based on chronic**
24 **continuous recordings of biomarker neural activities.** In this particular example, the
25 memory performance and the biomarker are quantified as the mean number of words recalled
26 in a verbal memory task and the rate of electrographically detected seizures, respectively.
27 DES with electrical currents at low or high frequency was used for a period of up to 2 years.
28 The study showed an overall enhancement in verbal memory performance of approx. 50%
29 and different effects of the two stimulation types. The model on the right summarizes an
30 example profile of biomarker and behavioral responses to three different DES patterns with
31 the former preceding the latter. Adapted from Marks et al. 2022.

32

1 **Table 1 Basic classification of DES approaches applied for modulation of memory and cognitive functions**

Category	Mode	Responsive?	Example use	Example study
Continuous	Chronic	No	DES permanently switched ON	Hamani <i>et al.</i> ³⁸ Laxton <i>et al.</i> ⁴⁴ Troster <i>et al.</i> ¹⁰⁷
Phasic	Chronic	No	DES switched ON manually during active cognition	Fell <i>et al.</i> ⁴² Koubeissi <i>et al.</i> ⁴⁰ Miller <i>et al.</i> ⁴³
Phasic	Chronic	Yes	DES switched ON by automated state detection	Bergey <i>et al.</i> ¹⁰⁵ Nair <i>et al.</i> ¹⁰⁶
Phasic	Acute	No	Open-loop DES triggered by a cognitive event	Suthana <i>et al.</i> ³¹ Inman <i>et al.</i> ⁷¹ Kuciewicz <i>et al.</i> ²⁴
Phasic	Acute	Yes	Closed-loop DES triggered by feedback from brain activities	Ezzyat <i>et al.</i> ²⁵ Hampson <i>et al.</i> ⁷⁵

2
3 Adaptive stimulation is not classified separately here as it is more general and can employ a number of the listed stimulation
4 approaches.

5 **Box 1 The complexity of memory functions**

6 Which memory function should be targeted by DES? Traditionally, declarative memory
7 processes have been separated into memory encoding, storage (or maintenance),
8 consolidation, and retrieval. These processes are likely to depend on very different and
9 possibly even opposing neurophysiological processes (e.g.,⁷⁻⁹, which may lead to
10 interference between encoding and retrieval¹⁰. Thus, a DES pattern that improves initial
11 memory formation (encoding) may actually impair consolidation and/or retrieval. One
12 possibility to overcome this problem is asking the patient to intentionally select whether they
13 want to encode or retrieve information in a given setting. Alternatively, some external
14 information may be used to select the memory “mode” that is most likely relevant in a given
15 situation (e.g., enhance encoding during explorative behavior and movement, facilitate
16 retrieval during rest, and boost consolidation during sleep).

17 A further level of complexity is that declarative memory is only very crudely conceptualized
18 as a pure storage device but needs to enable flexible access to specific aspects of an episode
19 (e.g., either its perceptual or its semantic aspects). Furthermore, memories need to be
20 connected and integrated in order to usefully guide behavior: A mere collection of
21 disconnected individual episodes is not particularly helpful, but they should be organized into
22 hierarchical knowledge structures. This also implies that memories should undergo
23 transformations, in particular semanticization (e.g.,^{11,12}. DES may attempt to support such
24 memory transformation processes, e.g., by strengthening semantic representational formats in

1 memory. A challenge is that this may come at the expense of reduced memory for perceptual
2 details.

3 Not every event we encounter should be stored in memory. Not only do we want to filter out
4 irrelevant details, but also be able to forget emotionally distressing events. The relevance of
5 this “positivity bias” for mental wellbeing – which may occur at the level of encoding,
6 consolidation, or retrieval – has often been described. And if unwanted information has been
7 encoded, it is often still possible to purge it from our memories via deliberative and
8 intentional forgetting¹³. Inhibitory control over memory is highly relevant for mental health
9¹⁴, but how it should be considered in DES for memory remains an open question.
10 Modulation of the higher order executive brain functions is one possibility.

11 Finally, it is still an open question how we measure an improvement of memory outside of
12 the lab, i.e. when stimuli are not experienced one after the other but in a continuous stream,
13 and often actively sampled by our goal-behavior. Which events does a person in this natural
14 environment even want to remember? An ecologically valid measure of memory and its
15 impairment may be to use experience sampling methods like mini-surveys or self-reports, and
16 to inquire how often patients experienced subjective memory failure. This can be done
17 concurrent with the new technologies for continuous recording and stimulation (see also
18 below ‘A new perspective for modulating memory and cognition’) that are even capable of
19 automatically inquiring cognitive states based on neural activity biomarkers (see also below
20 ‘Biomarkers of neuromodulation’).

21

22

1 **Box 2 Overview of non-invasive brain stimulation approaches**

2 The most prominent non-invasive brain stimulation methods that could be applied in humans
3 are transcranial magnetic stimulation (TMS), transcranial electric stimulation (TES) and,
4 more recently, focused ultrasound (FUS). In addition, vagus nerve stimulation (VNS) is a
5 semi-invasive method that has been applied in several psychiatric diseases as well as in
6 pharmacorefractory epilepsy patients with contraindications for resective surgery (e.g.,
7 because of bilateral hippocampal lesions).

8 TMS and TES can be either used to excite or to inhibit brain regions, depending on
9 stimulation parameters. Both of them have relatively limited penetration depth, i.e., they are
10 limited in their abilities to target deep brain regions such as the hippocampus. However, some
11 attempts in this direction have been made, and it is possible to non-invasively enhance
12 cortical-hippocampal networks and memory performance, as shown in a study using TMS to
13 parietal regions to exert indirect influences on hippocampal activity and function ⁶⁰.

14 While it has been argued that TMS effects are relatively artificial because of the large
15 magnetic fields that are induced, TES stimulation may be more physiological. This is
16 particularly the case for TES with alternating (oscillatory) currents, i.e. transcranial
17 alternating current stimulation (tACS). TACS may be selectively effective by increasing
18 endogenous subthreshold oscillations, a mechanism known as "entrainment" (for a review,
19 see ⁶¹).

20 In addition to these relatively established methods, a more recent approach consists in the
21 delivery of ultrasonic stimulation via focused ultrasound (FUS; for a recent review, see
22 e.g. ⁶²). Again, depending on stimulation parameters, FUS may be both excitatory and
23 inhibitory; in addition to its application at high intensity for resective surgery, low-intensity
24 FUS can be safely used to exert reverse effects on brain functioning (e.g., see ⁶³) and may be
25 a potential treatment option for memory dysfunction in Alzheimer's disease (e.g., ⁶⁴).

26

27

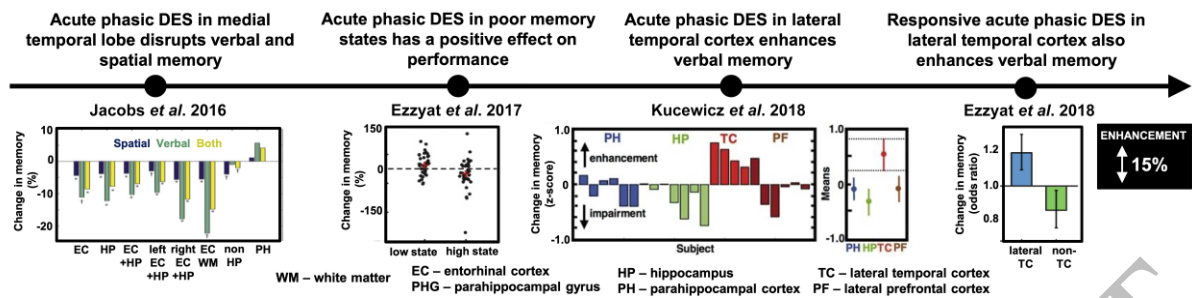


Figure 1
159x38 mm (x DPI)

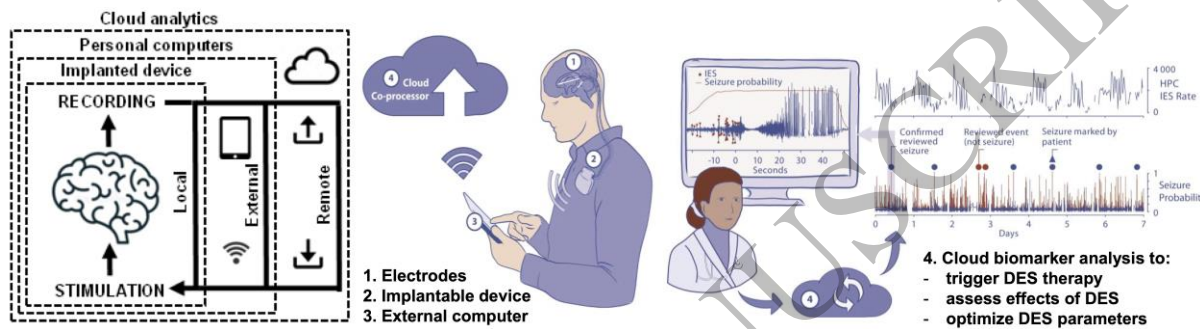


Figure 2
159x43 mm (x DPI)

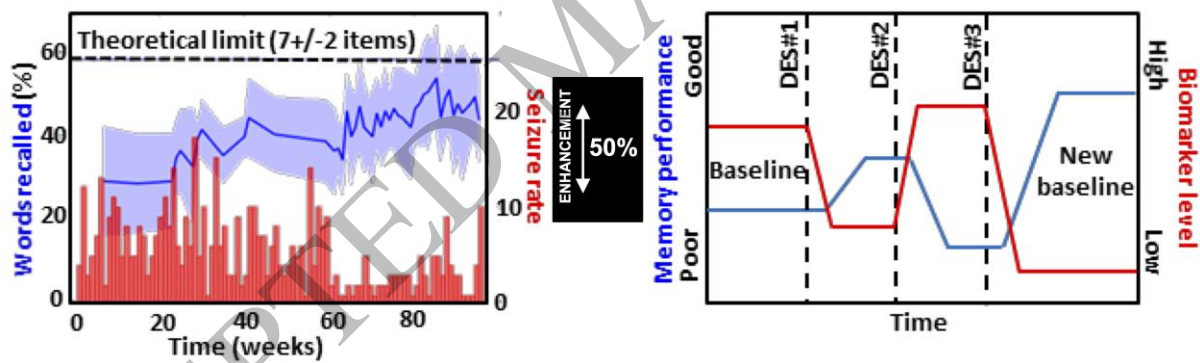


Figure 3
159x48 mm (x DPI)